

OBJECTIVE PERCEPTUAL QUALITY ASSESSMENT FOR SELF-STEERING BINAURAL HEARING AID MICROPHONE ARRAYS

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Introduction

- A novel **self-steering beamformer with binaural output** for a head-worn hearing aid microphone array is presented.
- Direction of arrival estimation (DOA) and noise reduction including several different head models
- Performance evaluation and test in a **realistic sound scenario using real-world recordings**
- **Benchmark test** for multi-channel noise reduction schemes with binaural output using **objective quality measures based on perceptual models of the auditory system** is proposed for performance evaluation.

Binaural Noise Reduction

- Minimum variance distortionless response (MVDR) beamformers with binaural output stage are promising for hearing aid applications.
 - Spatial information can still be exploited by the listener
 - Target signal direction estimation is needed ⇒ DOA estimation

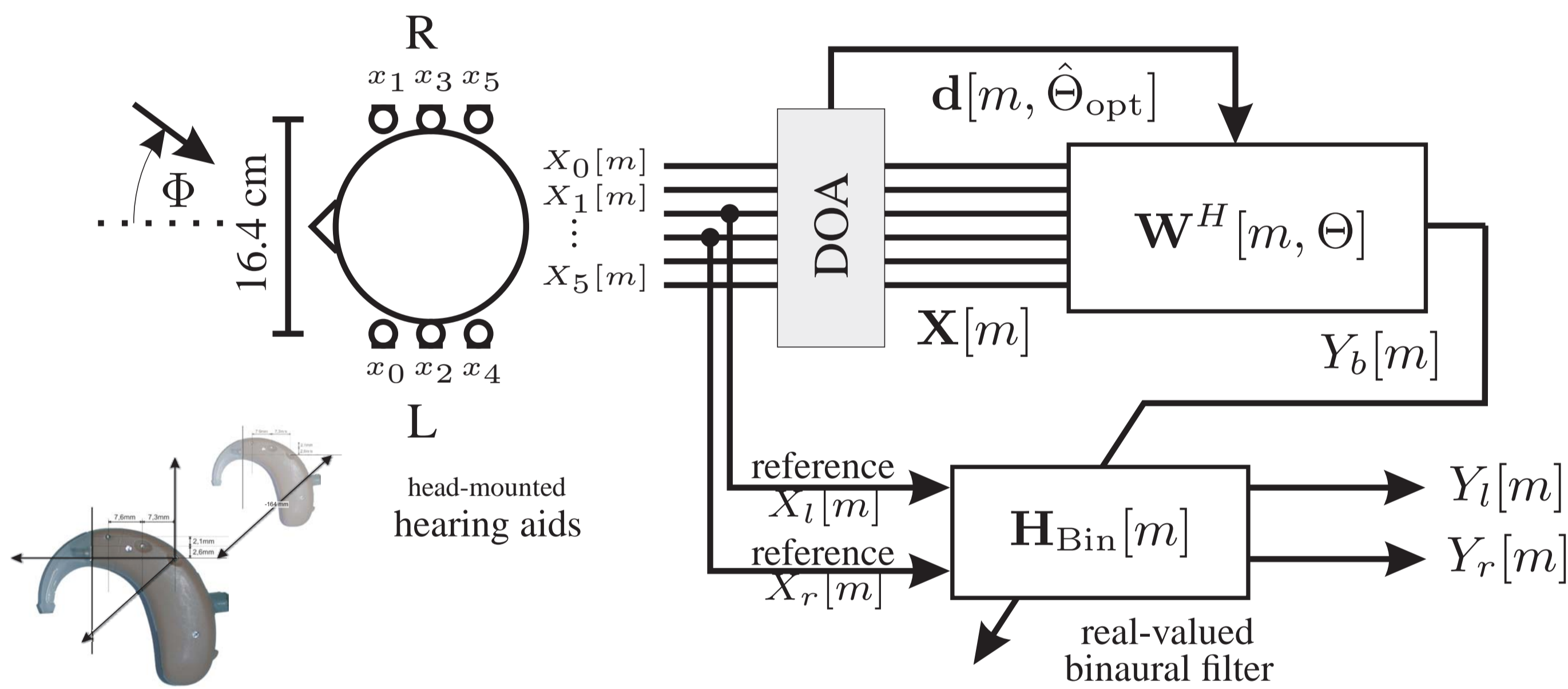


Fig. 1. 6-channel beamformer with head mounted microphone array, DOA estimator and binaural post-filter

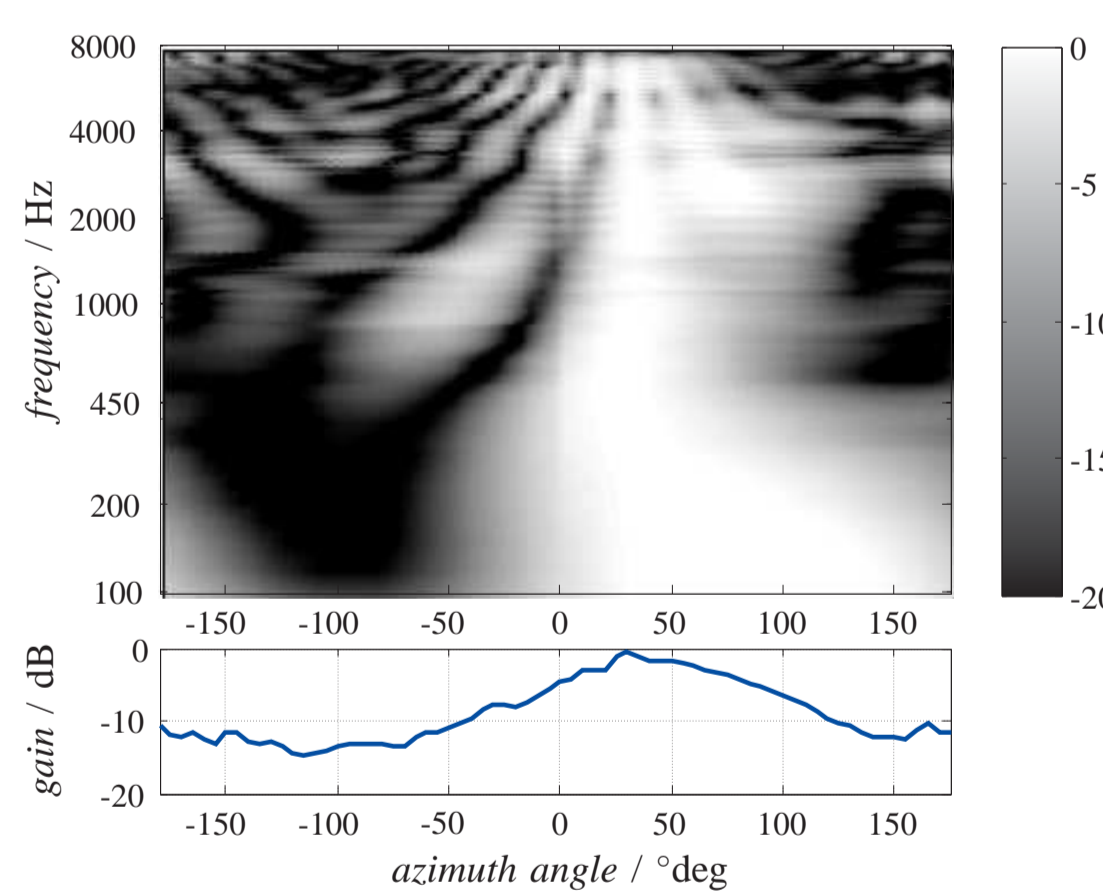


Fig. 2. Beampattern for a 6-channel beamformer as seen on the head

- Classical MVDR beamformer [9, 10]

$$\mathbf{W}[m, \Theta] = \frac{\mathbf{\Gamma}_{NN}^{-1}[m] \mathbf{d}[m, \Theta]}{\mathbf{d}^H[m, \Theta] \mathbf{\Gamma}_{NN}^{-1}[m] \mathbf{d}[m, \Theta]}$$

$$\mathbf{d}[m, \Theta] = [d_0[m, \Theta], d_1[m, \Theta], \dots, d_{N-1}[m, \Theta]]^T$$

$$d_i[m, \Theta] = |d_i[m, \Theta]| e^{-j2\pi m \frac{d_i}{M} \tau_i[m, \Theta]}, \quad i = 0..N-1$$

- Binaural output stage adapted from [5]

$$H_{\text{Bin}}[m] = \frac{(|d_l[m, \Theta]|^2 + |d_r[m, \Theta]|^2) \Phi_{Y_b Y_b}[m]}{\Phi_{X_l X_l}[m] + \Phi_{X_r X_r}[m]}$$

$$Y_l[m] = H_{\text{Bin}}[m] X_l[m]$$

$$Y_r[m] = H_{\text{Bin}}[m] X_r[m]$$

Signals

- Head related transfer functions (HRTFs) were recorded in anechoic room and in an office environment.
- 3 different signal mixes were evaluated:

	Noise Field	Moving Speaker
Condition 1:	Diffuse noise	anechoic HRTF
Condition 2:	Office noise	Office HRTF
Condition 3:	Cafeteria noise	Office HRTF

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Direction of Arrival Estimation (DOA)

- DOA estimation is based on the Generalized Cross Correlation approach (GCC-PHAT) [11]

$$\tau_d = \arg \max_k R_{x_l x_r}[k]$$

$$R_{x_l x_r}[k] = \frac{1}{L_{\text{DFT}}} \sum_{m=0}^{L_{\text{DFT}}-1} \frac{\Phi_{x_l x_r}[m]}{|\Phi_{x_l x_r}[m]|} e^{j \frac{2\pi}{M} m k}$$

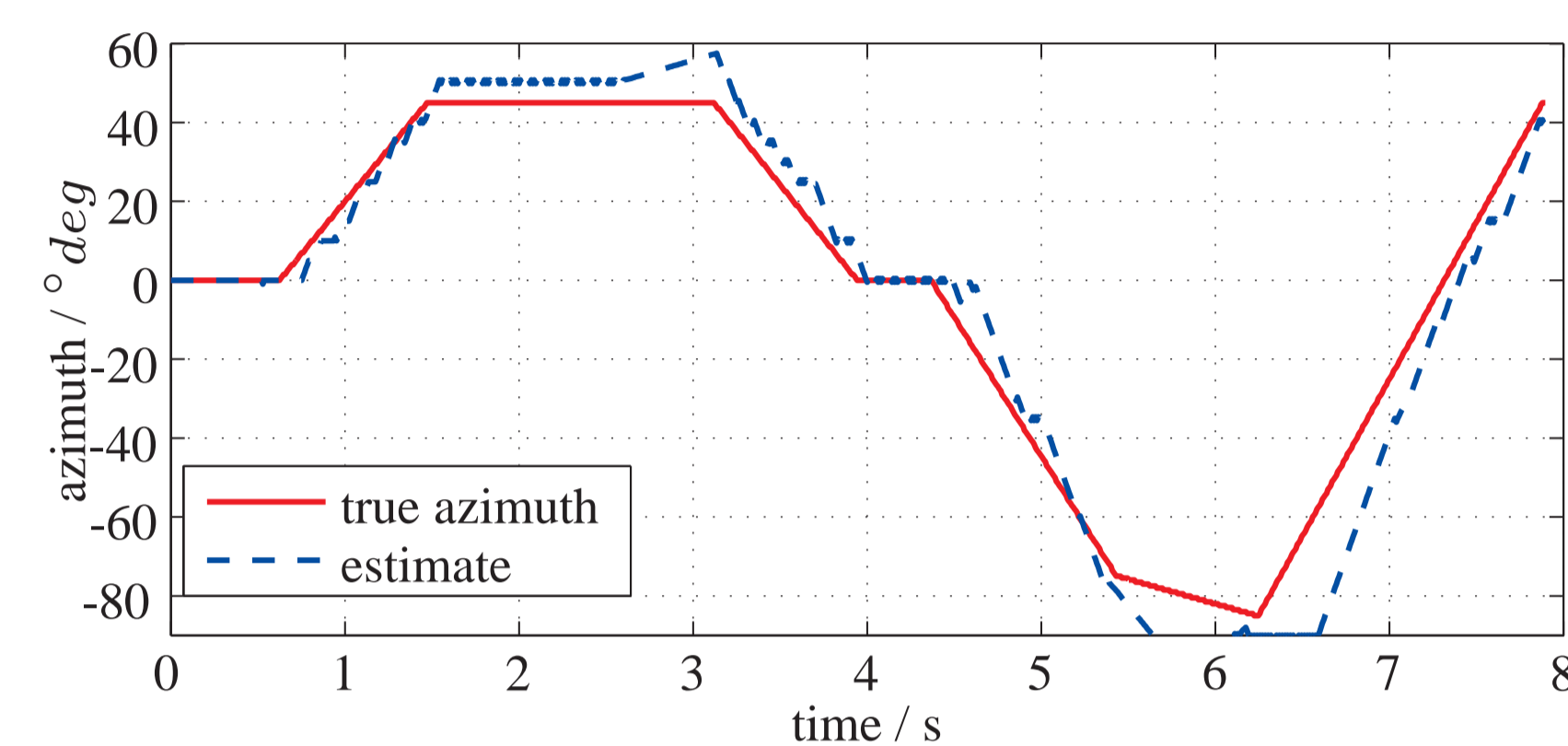


Fig. 3. Virtual azimuth path of a moving speech source and its estimate for HM2 at 12dB SNR. The movement is simulated by time variant filtering of the signal with HRTFs from different directions.

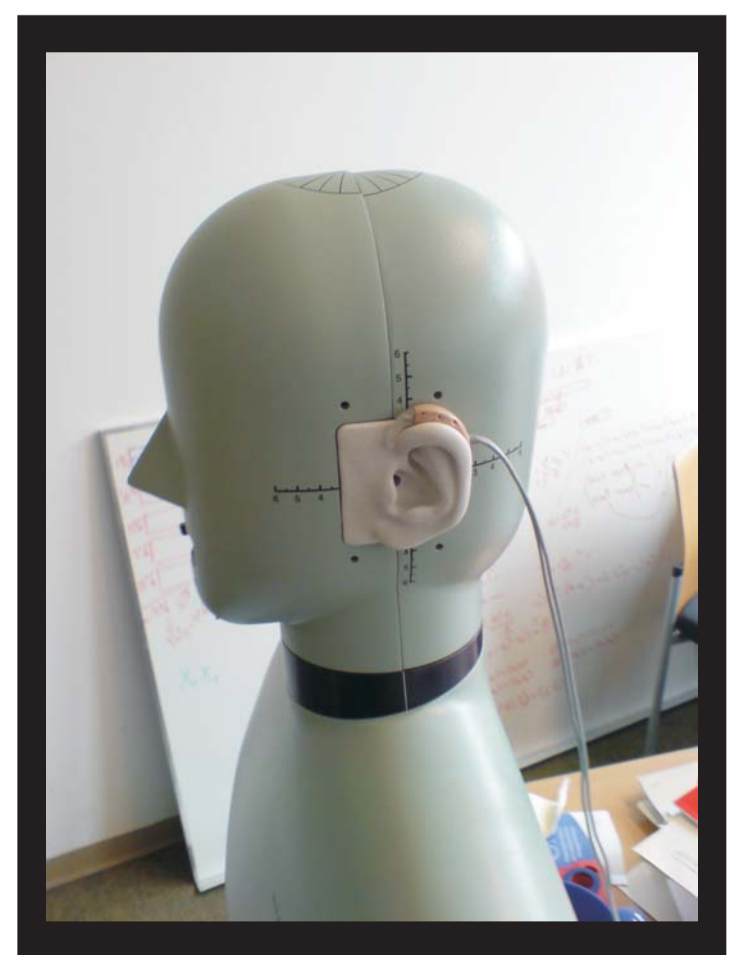


Fig. 4. HRTF Measurements

Propagation Models

- Binaural cues for DOA estimation with head-worn microphone arrays:
 - Interaural level difference (ILD)
 - Interaural time difference (ITD)
- HRTFs should be incorporated into design of DOA estimator (HRTFs user dependent ⇒ head models)

Head Models

- Head models incorporate both, changes of ILD and ITD, due to head shadow and diffraction effects. (Two head models were evaluated HM1 [12] / HM2 [13])
- Interaural Time Difference (ITD)

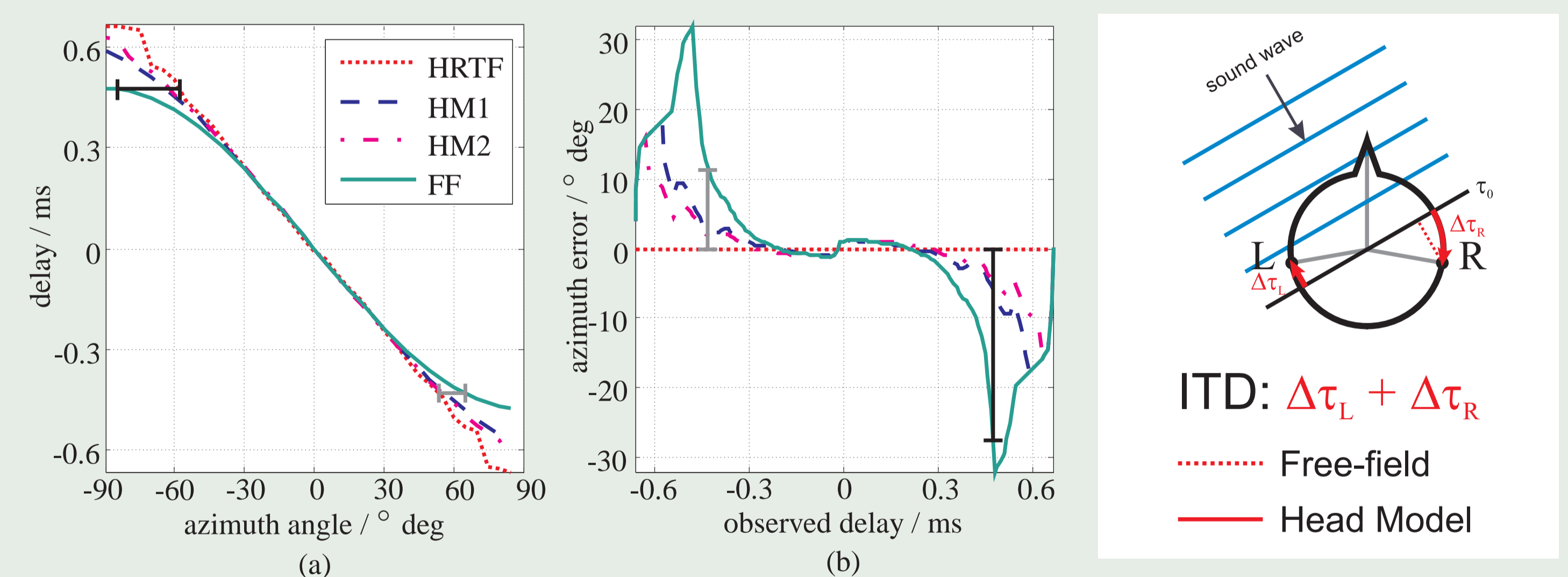


Fig. 5. Comparison of interaural time differences for free-field assumptions, HRTFs, and head models (HM1 / HM2)

- Interaural Level Difference (ILD)

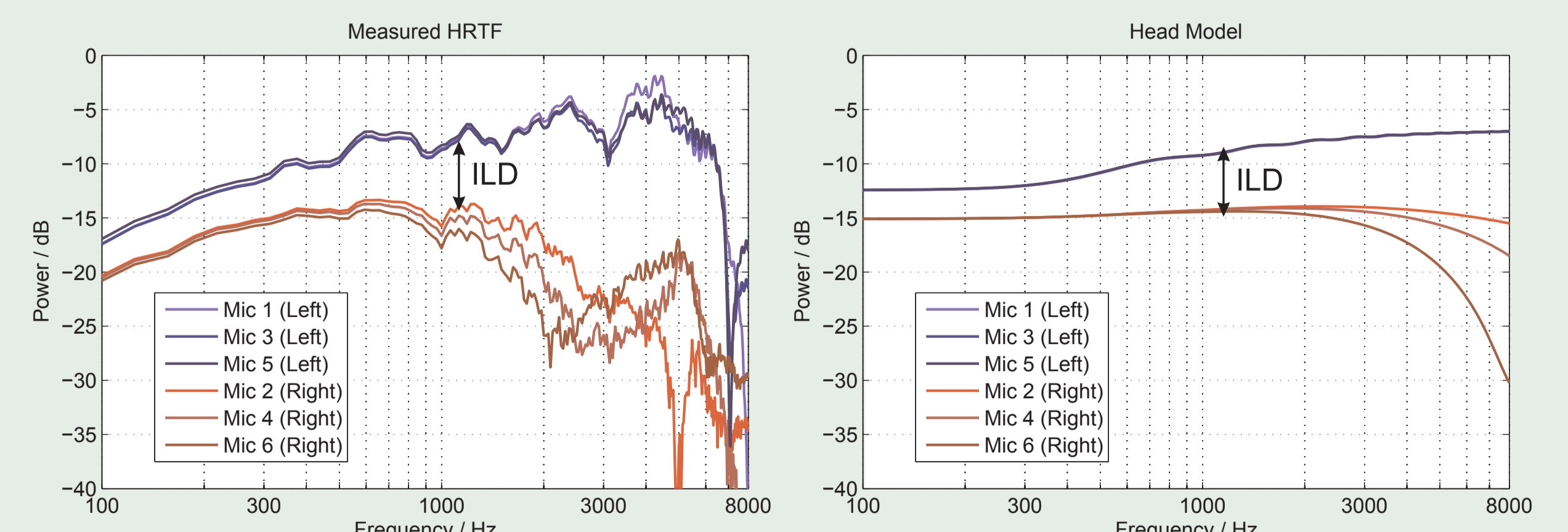


Fig. 6. Comparison of interaural level differences for HRTFs (left) and head models (right, HM2)

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Results

DOA Estimation Error

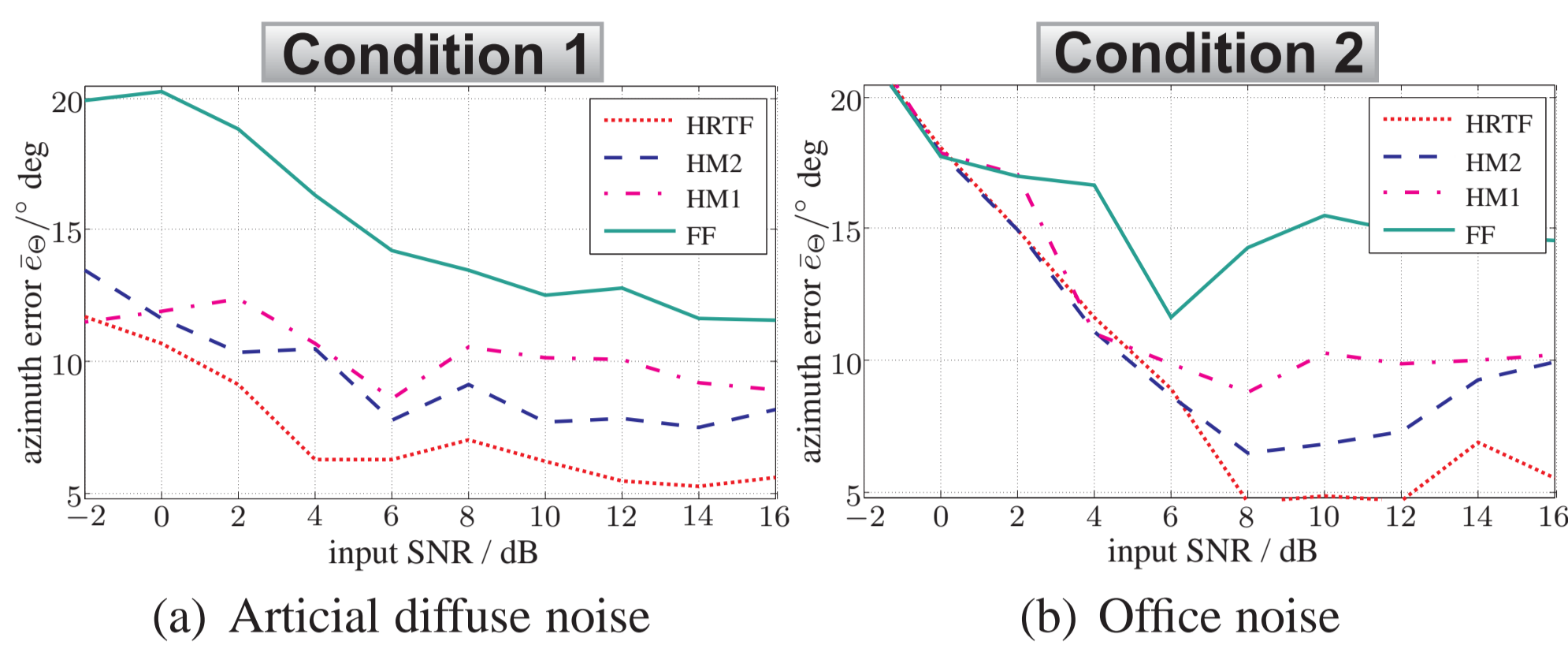


Fig. 7. Average error of the direction of arrival (DOA) estimation in different noise conditions.

Overall Quality

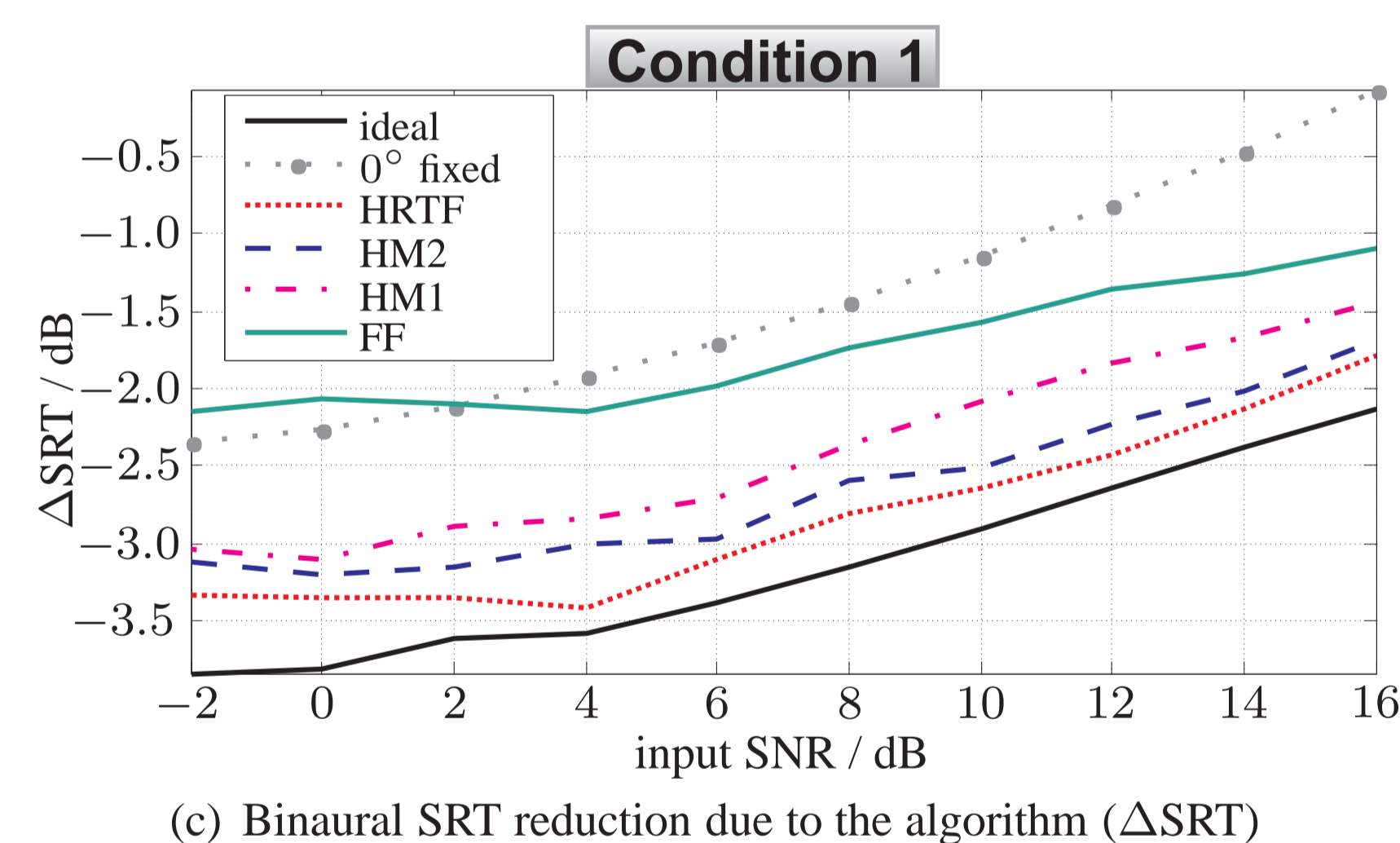
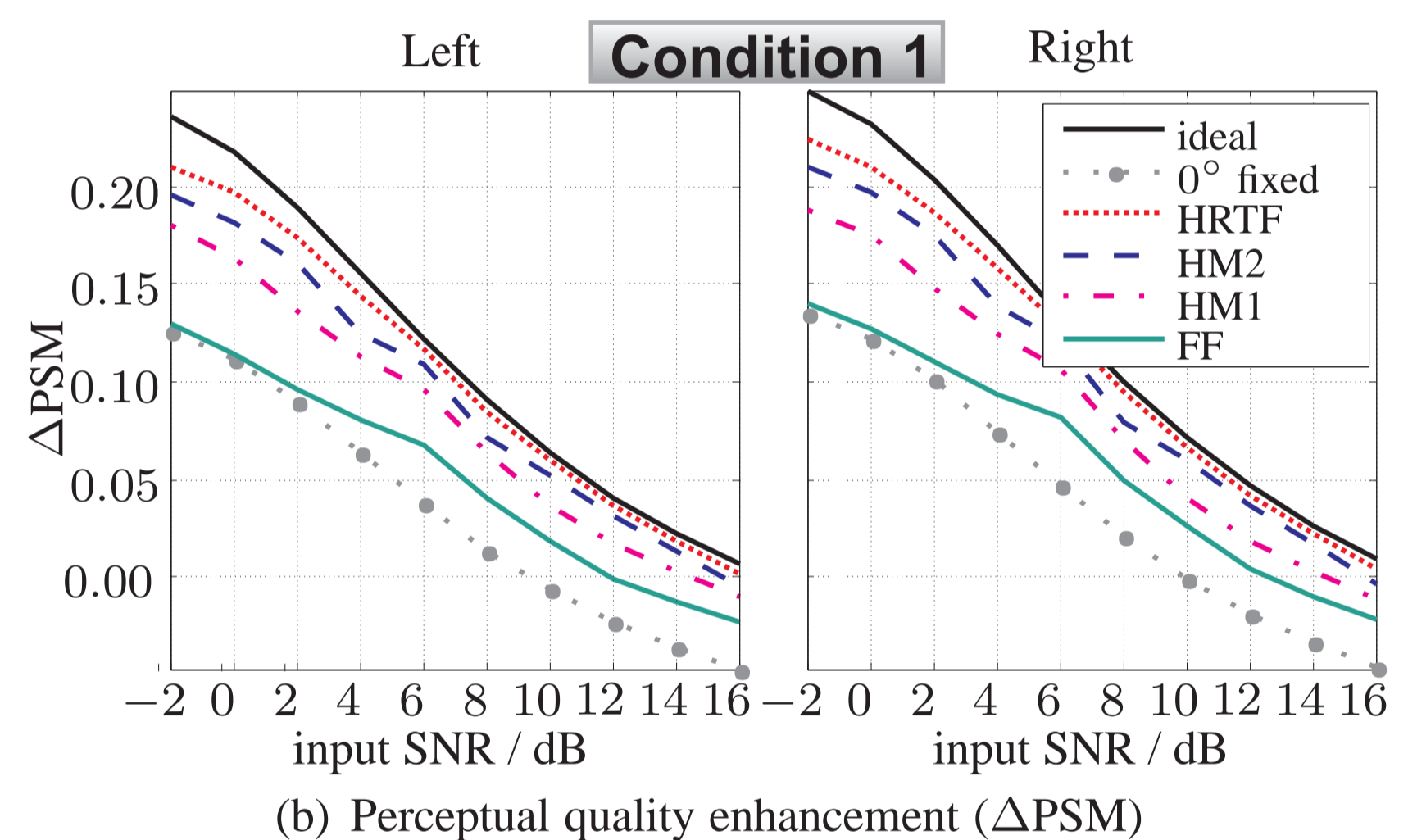
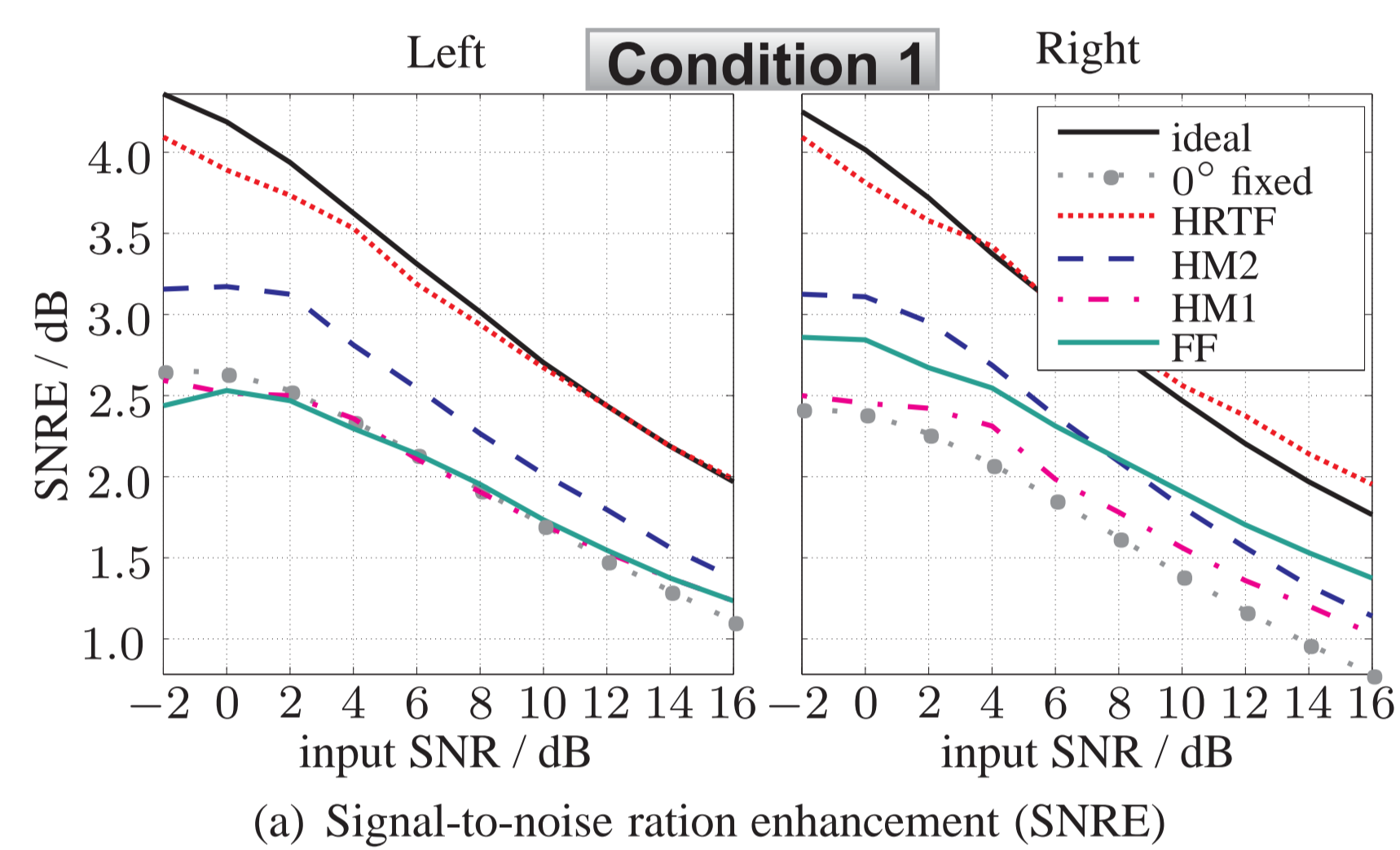


Fig. 8. (c)-(d) Objective binaural Δ SRT measure shows the expected gain in speech intelligibility due to noise reduction and

- Depending on the directivity $\bar{e}_0 < 10^\circ$ deg is an acceptable value.

- At least a coarse head model is needed.

Fig. 8. (a)-(c) Objective quality assessment of DOA plus beamformer system with different propagation models in artificial diffuse noise. Ideal system has a priori information about the direction of arrival and uses the measured HRTF as a propagation model.

The 0° fixed system uses the measured HRTF for beamforming but the DOA is fixed to the look direction (0° deg).

preservation of binaural information. A lower Δ SRT leads to a higher speech intelligibility. (d)+(e) show the performance results in

difficult noise conditions: still the self-steering systems that include at least a coarse head model are superior to the fixed system.

Quality Measures

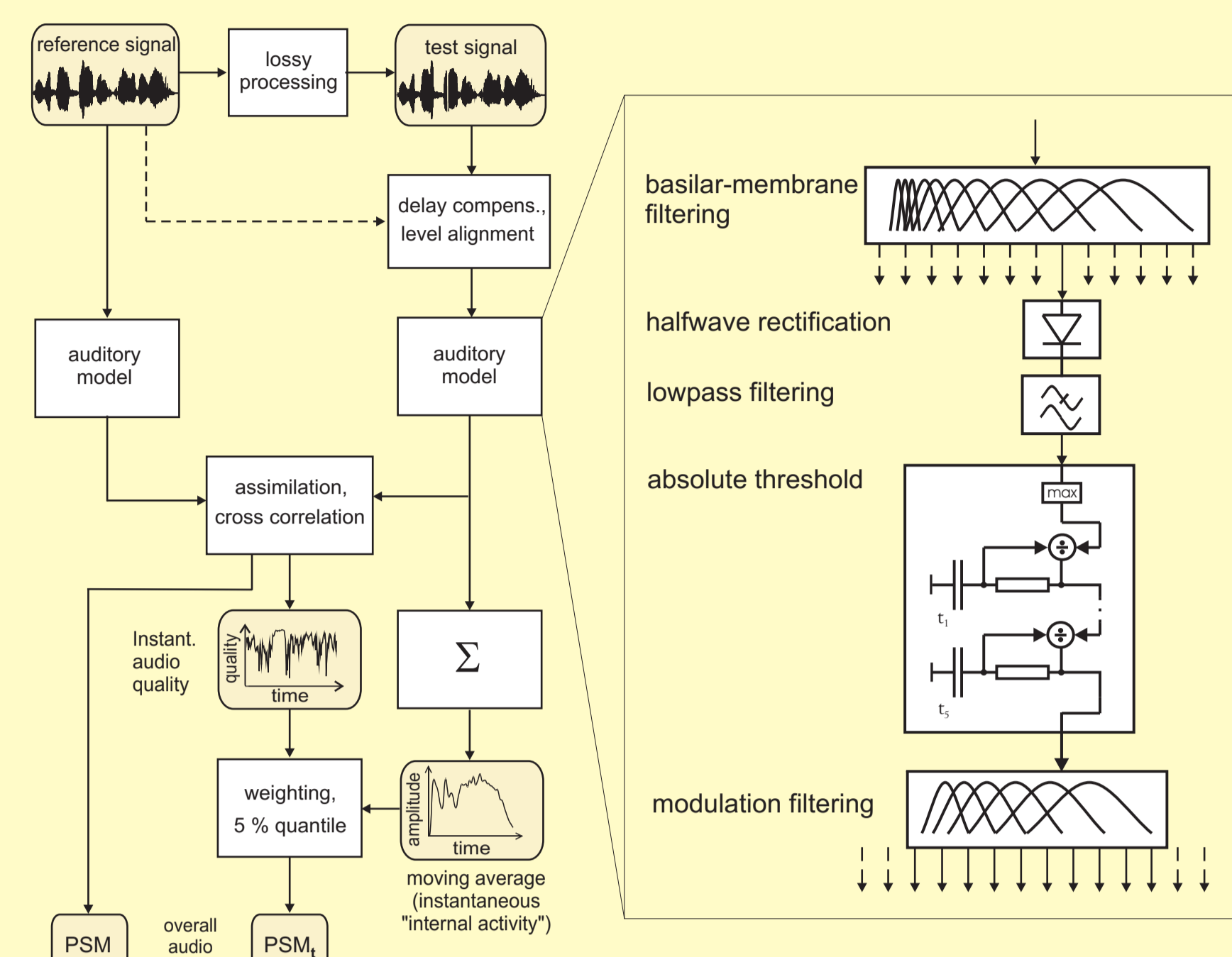


Fig. 9. The quality prediction method PEMO-Q [2]

- Objective performance evaluation is realized in a simulation system with the *shadow filtering* method (i.e. signal and noise are processed separately using the filter coefficients as calculated for the mix).

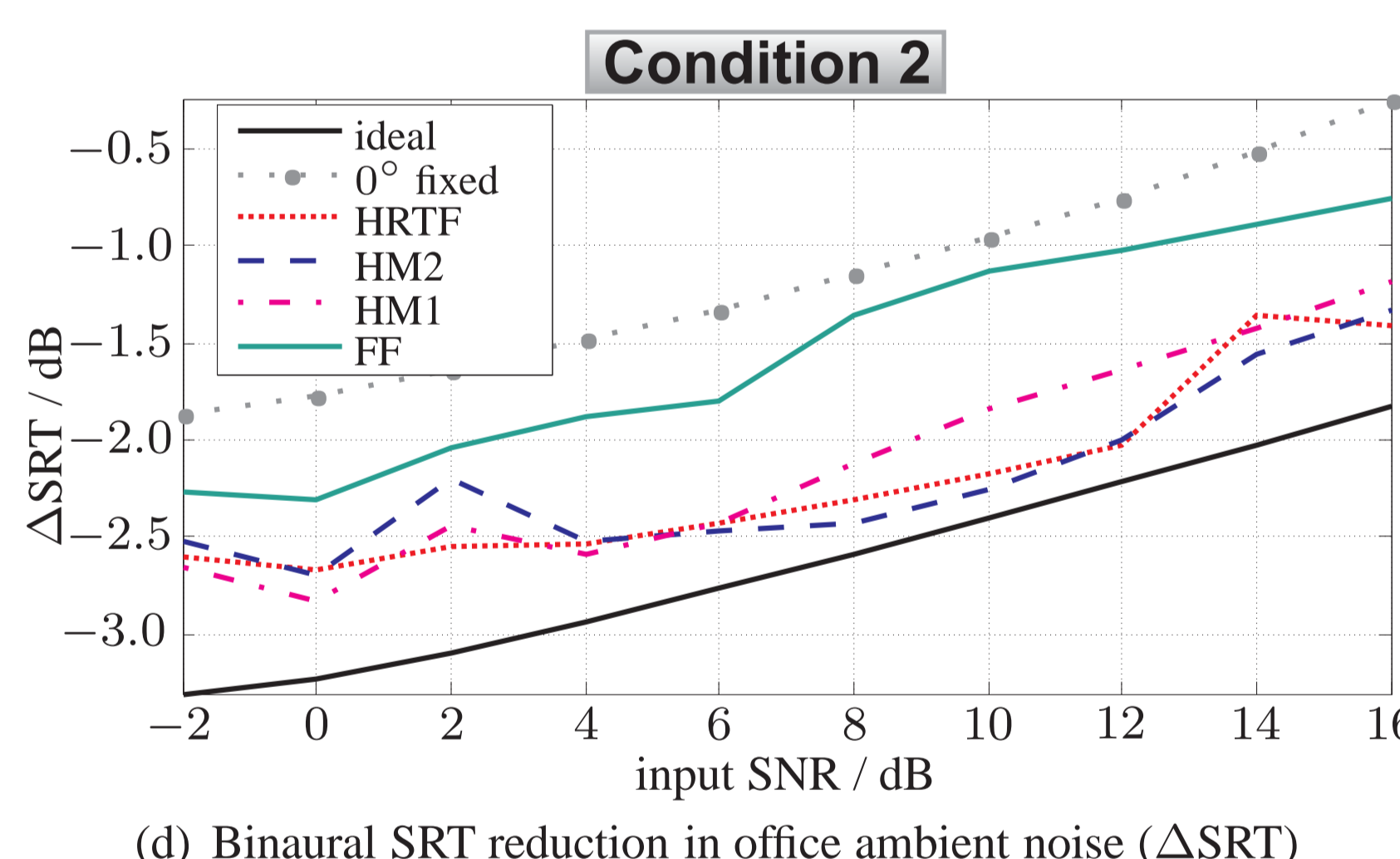
- Signals can be transformed by models of auditory perception and are compared in the internal representation domain.

- Individual hearing loss can be integrated into auditory models.

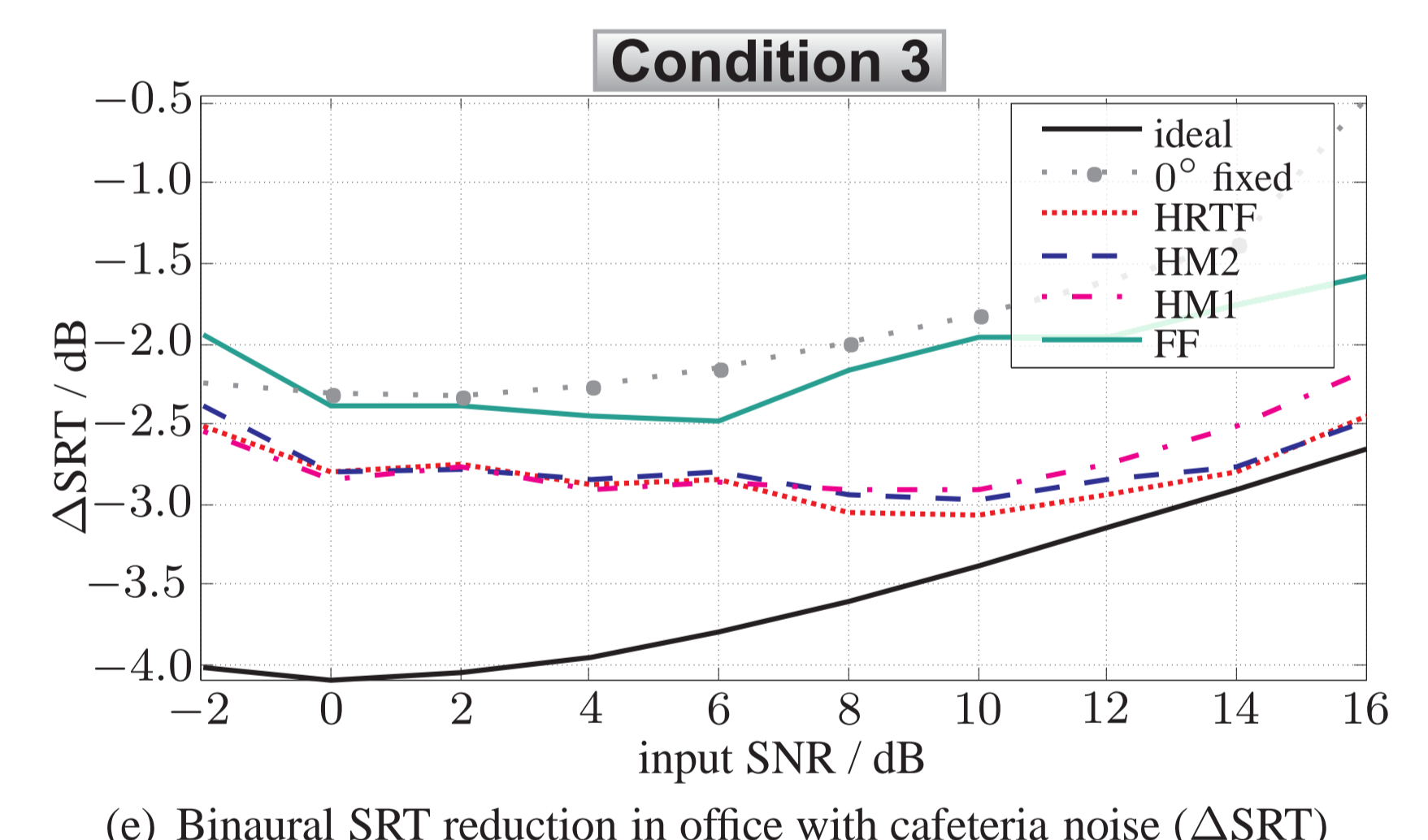
- The SNR-Enhancement (SNRE) is the difference of the signal-to-noise ratio (SNR) at the output of the noise reduction system and a reference input SNR, both measured in dB. For binaural systems the SNRE must be calculated bilaterally. By simply taking the average SNRE, the better-ear effect would be ignored.

- The quality measure PSM from PEMO-Q [2] estimates the perceptual similarity between the processed signal and the clean speech source signal. For monaural noise reduction schemes this measure has shown a high correlation with subjective overall quality ratings according to [1,14]. For binaural outputs PSM is measured bilaterally [16].

- The speech reception threshold (SRT) is defined as the SNR at 50% speech intelligibility. In [3] a binaural model of speech intelligibility based on the equalization cancellation (EC) processing by Durlach had been defined which is able to predict the SRT with high accuracy. Here, we are interested in the Δ SRT, i.e. the difference between input and output SRT. The binaural speech intelligibility measure provides an integrative measure of binaural unmasking and can identify differences in the estimated speech-reception threshold (SRT) if binaural information is distorted [16].



(d) Binaural SRT reduction in office ambient noise (Δ SRT)



(e) Binaural SRT reduction in office with cafeteria noise (Δ SRT)

Conclusion

- Self-steering beamformer for the application in a binaural hearing aid system shows promising results.
- Performance evaluation under realistic conditions is only reliable using perceptual models of the auditory system [1,16].
- The results show the importance of the propagation model for the DOA estimation and beamforming on a head-worn binaural system.

- The DOA-beamformer system performs best in diffuse or office noise conditions. In adverse noise conditions, such as cafeteria noise, the achievable performance gain is lower compared to a system with perfect knowledge about the direction of arrival.
- For signal-to-noise ratios greater -2dB self-steering systems are superior to systems that assume a fixed look direction if a certain complexity of the propagation model is met.
- The individual HRTFs are not needed, head models are sufficient.

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